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ORIGINAL ARTICLE

Effect of capsaicin-sensitive sensory neurons on bone architecture and mechanical properties in the rat hindlimb suspension model



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KEYWORDS bone; capsaicin; hindlimb suspension; sensory neuron Summary Background/Objective: The participation of sensory neural regulation in bone metabolism has been widely studied. However, the physiological role of sensory neural regu- lation in the functional adaptation to weight bearing is not clear. This study was conducted to investigate the effect of capsaicin-induced sensory neuron lesions on cancellous architec- ture properties in a hindlimb suspension (HLS) model. Methods: Thirty-two female rats were randomly assigned to four groups. Groups b and d under- went systemic capsaicin treatment, whereas Groups a and c were treated with vehicle. Then, Groups c and d were subjected to HLS, whereas Groups a and b were allowed hindlimbs full loading. The proximal trabecular and mid-shaft cortical bone structure were evaluated via mi- crocomputed tomography, and the biomechanical properties of the tibial mid-shaft were as- sessed using the four-point bending test. Results: The trabecular bone volume was reduced by 40% and 50% in Groups b and c, respec- tively, and was also reduced significantly in Group d. Trabecular thickness and trabecular sep- aration in Group b were not significant difference among all groups. Compared with Group a, the ultimate strength in Group b decreased by 20.3%, whereas it did not change significantly in Group c. Conclusion: The results suggest that capsaicin-sensitive sensory neurons play an important role in bone modelling. The effect of capsaicin is similar to HLS. However, HLS has no add-on effect to capsaicin in the reduction of bone density and mechanical properties.		
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Translational potential of this article: This study gives clues to the function of sensory neurons in bone modelling.

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Introduction

It has been demonstrated that bone tissue is highly sensitive to mechanical stress and can change its shape, structure, and mineral density. The mechanism of bone loss due to immobilisation, paralysis, long-term bed rest, and spaceflight, and the mechanism of bone mass increase owing to regular resistance exercises indicate that bone turnover is sensitive to both external loads arising from gravitational loading and to internal loads generated by muscle activity [1,2]. The ability of bone to sense the mechanical stimuli was considered to be a local interaction between the loading and the affected bone cells [3]. However, the participation of neural regulation has been demonstrated in both local and systemic bone metabolism based on the innervation of the sympathetic and peripheral sensory neurons in bone via osteoblastic and osteoclastic cell guidance [4-6]. Substance P (SP) and calcitonin generelated peptide (CGRP), which are important neuropeptides, are synthesised in unmyelinated sensory neurons, which are the target of capsaicin, and released from their peripheral terminals [7]. It has been demonstrated that bone integrity was compromised by decreased levels of local neuropeptide in bone in some hereditary sensory neuropathies, such as familial dysautonomia [8,9]. The innervation of the developing mouse femur was guided by nerve growth factor-neurotrophic tyrosine kinase receptor type 1 signalling, in turns, to promote vascular invasion of the ossification centres and osteoprogenitor cell lineage progression [6].

Capsaicin is the major pungent component of hot chili peppers. Transient receptor potential (TRP) vanilloid subfamily member 1 (TRPV1) is identified as the receptor of capsaicin [10]. TRPV1 is expressed in unmyelinated and small-diameter myelinated sensory neurons [11]. The activation of TRPV1 by capsaicin induces Ca²⁺ and Na⁺ influx into the sensory neuron, causing an excitotoxic effect. Large sensory neurons, motor neurons, and sympathetic neurons are affected by lack of vanilloid receptors [12,13]. It has been demonstrated that only the unmvelinated and small-diameter myelinated sensory neurons are destroyed when capsaicin is administered in neonatal rats, whereas the large sensory afferent, motor, and sympathetic fibres are unaffected [14,15]. Capsaicin treatment could deplete SP and CGRP in peripheral nerves, but not in the central nervous system [16,17]. The depletion rate of the unmyelinated fibres in adult rat induced by capsaicin injection has been reported to reach 90-95% [18]. In addition, systemic capsaicin treatment of the adult rat results in the death of at least 50% of the vagal afferent neurons in dorsal root ganglia [19].

Mechanical stimulation influences bone metabolism. However, will there be any difference in the response if the sensory nerve fibres in bone tissue are partially or completely destroyed? The aim of this study is to investigate the role of capsaicin-sensitive sensory neurons in bone modelling in a rat hindlimb suspension (HLS) model. In this study, the unmyelinated sensory fibres were depleted by systemic capsaicin treatment under a functional disuse HLS condition. The bone structure and biomechanical properties of the rat tibia were evaluated to assess the bone response to loading changes after capsaicin treatment.

Materials and methods

Animals

The *in vivo* experiment was approved by the Institutional Animal Care and Use Committee (IACUC), Stony Brook University (Stony Brook, NY, USA). Thirty-two 4-month-old female Sprague—Dawley rats weighing 245 ± 15 g were used in the study. The animals, which were randomly assigned in equal numbers (n = 8) to four groups, received different interventions as follows: Group a, control; Group b, capsaicin only; Group c, HLS only; Group d, combination (HLS after capsaicin treatment). All animals were raised in separate cages in a temperature-controlled room ($22^{\circ}C$) with a 12:12-hour light—dark cycle. Standard rodent chow and water were provided *ad libitum* throughout the experiment. All experimental procedures were in accordance with the IACUC guidelines.

Capsaicin treatment

The rats were injected subcutaneously in the back with capsaicin (Sigma, St. Louis, MO, USA). To prevent reflux from the needle tract, the needle was left in the skin for 60 seconds after the injection. The capsaicin treatment protocol consisted of three injections. The initial one was 25 mg/kg, the second one was 50 mg/kg at 6 hours later, and the third one was 50 mg/kg at 24 hours after the first injection [20]. To prevent pulmonary oedema, all rats in the capsaicin treatment groups (Groups b and d) had no water supply 6 hours prior to the capsaicin injection [21]. The protocol was repeated every 2 weeks (Weeks 1, 3, 5, and 7), and all experiments were performed during Weeks 5 to 8. The groups without capsaicin treatment (Groups a and c) underwent the same injection protocol with vehicle (10% Tween 80, 10% ethanol and 80% saline).

Hindlimb suspension

The rats in Groups c and d were hindlimb suspended for 4 weeks during Weeks 5 to 8 following established procedures [22]. Briefly, the animal's tail was cleaned with 70% ethanol and coated with tincture of benzoin. Once the tail is dry and sticky, a strip of adhesive tape (15 cm \times 0.5 cm) was applied to the animal's tail. The tape was then attached to a swivel apparatus that was suspended from the top of the cage. An approximately 30° head-down tilt was set to prevent contact of the animal's hindlimbs with the cage bottom. The animal's forelimbs were allowed full access to the entire cage bottom.

Bone microarchitecture

All animals were sacrificed at the end of Week 8. The right tibia of each rat was removed and fixed in 70% ethanol. The proximal and midshaft tibial were scanned to evaluate trabecular and cortical microarchitecture using a microcomputed tomography system (µCT) (µCT 40; Scanco Medical AG, Basserdorf, Switzerland). The scanned region corresponded to a zone of 400 transverse slices below the growth plate of the proximal tibia and 200 transverse slices above the tibia-fibula junction. From the acquired data, the region of interest was delineated 1.5 mm below growth plate up to a height of 0.6 mm (50 slices) for trabecular bone and 1.0 mm above the tibia-fibula junction up to a height of 0.6 mm (50 slices) for cortical bone. For image smoothing purposes and to define the desired analysed objects, all images were evaluated using Gaussian filter, with specific sigma and support values of 0.1 and 1, respectively. To discriminate between bone and background, the threshold values for trabecular and cortical bone were 290 and 400, respectively. In trabecular bone, bone volume fraction (BV/TV), trabecular number (Tb.N; mm), trabecular thickness (Tb.Th; mm), and trabecular separation (Tb.Sp; mm) were evaluated. And cortical bone area fraction (Ct.A/TA) was evaluated to analyse the cortical bone structure.

Biomechanical test

After μ CT scanning, all tibiae were subjected to the fourpoint bending test to evaluate the biomechanical properties using the materials testing system (MTS Systems



Corporation, Eden Prairie, MN, USA) following the established procedure [23]. The tibia was placed on its lateral surface on two rounded supporting bars that were 20 mm from each other. A preload of 1 N was applied by lowering the upper bar. A constant displacement rate of 6 mm/min was applied until bone break (Figure 1). The maximum load (ultimate load), displacement at ultimate load, the slope in the linear region of the ultimate load (extrinsic stiffness), and the area under the curve until ultimate load (energy to ultimate load) were determined.

Statistical analysis

All data are presented as the means \pm standard error of mean, and the statistical analysis of the data from the μ CT and the four-point bending test was performed using a one-way analysis of variance (ANOVA) followed by Tukey's *post hoc* test. Statistical significance was considered when p < 0.05. SPSS 17.0 (SPSS Inc., Chicago, USA) was used to perform the data analysis.

Results

Bone microarchitecture

As shown in Table 1, one-way ANOVA showed that the effect of the intervention was significant in BV/TV (p = 0.003), (p = 0.001), Tb.Th (p = 0.011), and Tb.Sp Tb.N (p = 0.014), but not in Ct.A/TA (p = 0.325). Analyses using the Tukey's post hoc test indicated that BV/TV reduced significantly in Group b (40%, p = 0.039), Group c (50%, p = 0.003), and Group d (45%, p = 0.008) compared with the normal control group (Group a). Tb.Th reduced significantly in Group c (p = 0.012), but not in Group b (p = 0.190) and Group d (p = 0.070). Tb.Sp increased significantly in Group d (p = 0.025), but not in Group b (p = 0.184) and Group c (p = 0.183). The 3D reconstruction μ CT images (Figure 2) showed the different types of bone loss in Groups b and c; the trabecular bone loss in Group b was homogenous, whereas in Group c the bone loss was more severe in certain areas.

Biomechanical test

Table 2 shows the bone mechanical property parameters. One-way ANOVA showed that the effects of interventions were significant in ultimate load (p = 0.010), displacement (p = 0.008), extrinsic stiffness (p = 0.014), and energy to ultimate load (p = 0.013). Tukey's *post hoc* test indicated that compared with Group a, the ultimate load reduced significantly in Group b (20.3%, p = 0.023), whereas the ultimate load in Group c was not significantly changed (p = 0.830). The displacement increased significantly in Group d (48%, p = 0.012), whereas those in Groups b and c were not significantly changed. The stiffness of bones reduced significantly in Group b (20.9%, p = 0.030) compared with Group a. The energy to ultimate load in Group d was 68% (p = 0.006) higher than that in Group b.

Table 1 Bone microarchitecture of tibia.								
Group	BV/TV	Tb.N (mm)	Tb.Th (mm)	Tb.Sp (mm)	Ct.A/TA			
a: Control	$\textbf{0.40} \pm \textbf{0.04}$	$\textbf{8.46} \pm \textbf{0.58}$	$\textbf{0.08} \pm \textbf{0.005}$	$\textbf{0.12} \pm \textbf{0.009}$	$\textbf{0.994} \pm \textbf{0.001}$			
b: Capsaicin	$\textbf{0.24} \pm \textbf{0.02}^{\texttt{*}}$	$\textbf{6.28} \pm \textbf{0.35}^{\texttt{*}}$	$\textbf{0.07} \pm \textbf{0.003}$	$\textbf{0.16} \pm \textbf{0.011}$	$\textbf{0.993} \pm \textbf{0.003}$			
c: HLS	$\textbf{0.20} \pm \textbf{0.02}^{\textbf{**}}$	$\textbf{6.25} \pm \textbf{0.37}^{\texttt{*}}$	$0.06 \pm 0.001^{*}$	$\textbf{0.17} \pm \textbf{0.009}$	$\textbf{0.995} \pm \textbf{0.001}$			
d: $HLS + C$	$\textbf{0.22} \pm \textbf{0.03}^{\text{**}}$	$\textbf{5.88} \pm \textbf{0.45}^{\textbf{**}}$	$\textbf{0.06} \pm \textbf{0.004}$	$\textbf{0.18} \pm \textbf{0.015}^{\textbf{*}}$	$\textbf{0.994} \pm \textbf{0.001}$			

BV/TV = trabecular bone, bone volume fraction; Ct.A/A = cortical bone area fraction; HLS = hindlimb suspension; Tb.N = trabecular number; Tb.Sp = trabecular separation; Tb.Th = trabecular thickness.

* p < 0.05 compared with the control group.

** p < 0.01 compared with the control group.



Figure 2 Three-dimensional reconstruction of microcomputed tomography (μ CT) images of cancellous bone of proximal tibia in Groups a (control), b (Capsaicin), c (HLS) and d (HLS + Capsaicin).

Discussion

The results have shown that both capsaicin and HLS can result in dramatic bone loss according to the BV/TV data in the proximal tibia trabecular bone. Capsaicin treatment causes bone loss that was close to the magnitude of bone loss caused by HLS. However, interestingly, HLS after capsaicin treatment does not lead to a further decrease in bone density.

HLS is a model that causes mechanical unloading of the hindlimbs [24]. It has been reported that HLS results in large reduction in bone formation and cancellous bone loss in both sexes, and the mechanisms are similar in both sexes [25]. Mechanical strain [26] and fluid shear stress [27] are the two most commonly accepted mechanisms for coupling the loading with bone formation changes. The current theory about the mechanisms of bone reaction to mechanical stimulus considers that mechanical strain to the cell membrane activates stretch-sensitive ion channels and other membrane-associated proteins such as integrins, which are involved in various cellular processes and structures [28]. According to the mechanostat theory, when the loading of bone is insufficient to produce bone strains that are above a minimum level of effective strain, bone mass and architecture are adjusted until bone strains are within the minimum effective strain range; as a result, bone resorption prevails over bone formation [29]. The fluid flow through cancellous bone and the lacuna canalicular network of cortical bone caused by mechanical loading exacerbates the flow-induced shear stress applied on surface bone cells [30]. Regardless of the mechanical strain or the fluid shear stress, bone cells respond through autocrine or paracrine signals that regulate remodelling process [31–33]. The cells detect the changes in fluid flow and physical deformation. Osteocytes and osteoblasts on the bone surface are the mechanosensors of bone. After a mechanical stimulus, these cells release prostaglandins and nitric oxide that promote bone formation and inhibit bone resorption, respectively [34]. Thus, when under an unloading situation, bone resorption is uncoupled from bone formation, contributing to the resultant bone loss.

Capsaicin, a neurotoxic agent, induces sensory denervation by inducing the death of most small dorsal root ganglion cells and leads to a loss of unmyelinated sensory axons [35]. Unmyelinated sensory neurons contain a variety

Table 2Biomechanical properties of tibia according to the four-point bending test.							
Group	Load (N)	Disp. (mm)	Stiffness (N/mm)	Energy (mJ)			
a: Control	$\textbf{99.0} \pm \textbf{6.6}$	$\textbf{0.68} \pm \textbf{0.09}$	176.9 ± 13.7	$\textbf{67.7} \pm \textbf{11.9}$			
b: Capsaicin	$78.9 \pm 1.6^{*}$	$\textbf{0.66} \pm \textbf{0.08}$	$140.0\pm8.6^{*}$	$\textbf{54.4} \pm \textbf{7.8}$			
c: HLS	101.5 ± 6.6	$\textbf{0.63} \pm \textbf{0.03}$	179.1 ± 10.6	$\textbf{65.3} \pm \textbf{7.5}$			
d: HLS+C	$\textbf{89.5} \pm \textbf{4.1}$	$\textbf{1.01} \pm \textbf{0.14}^{*}$	$\textbf{159.7} \pm \textbf{13.1}$	91.4 \pm 15.5**			

Disp. = displacement.

* p < 0.05 compared with the control group.

** p < 0.01 compared with the capsaicin group.

of transmitter peptides, such as CGRP and SP. CGRP has been reported to inhibit osteoclastogenesis [36] and bone resorption [37] and to stimulate osteoblasts proliferation and bone formation [38,39]. SP could stimulate osteoclast resorption and is involved in the pathogenesis of bone changes [40]. SP can both inhibit and stimulate bone formation in vitro [41,42], and the absence of SP reduces the bone formation rate in an adult model of endochondral ossification [43]. Some studies suggest that neuronal SP during bone regeneration has a role in bone formation, whereas during remodelling, increased SP fibre density in unloaded areas may be related to bone resorption [44]. However, because there are less SP-containing nerve fibres than CGRP-containing nerve fibres [45], the capsaicinsensitive sensory nerve fibres could be considered to be CGRP-positive nerve fibres. The depletion of CGRP-positive nerve fibres after regular capsaicin treatment inhibits bone formation and enhances bone resorption [46]. In the current study, the bone mass of tibia cancellous bone also decreased significantly after capsaicin treatment, even though the hindlimbs were fully loaded. This finding suggests that normal mechanical loading does not necessarily lead to normal balance of bone remodelling. HLS does not lead to additional bone loss after depletion of CGRPpositive nerve fibres by capsaicin treatment. A previous study [47] has demonstrated that sciactomy decreased the density of CGRP-positive nerve fibres in tibia fracture callus and resulted in low response of callus to ultrasound stimulation, which is well known in accelerating fracture healing in bone with normal innervations [48].

The μ CT result showed that Tb.Th in the HLS group was significantly lower than that in the control group, whereas Tb.Th in the capsaicin group was not significantly different from that of the control group. In addition, the 3D reconstruction μ CT image revealed the different types of bone loss in these two groups. The difference between the capsaicin group and the HLS group suggests that CGRP-positive nerve fibres may not be the only mechanosensors in bone. In addition, results from the biomechanical tests showing that the ultimate load of the capsaicin group was lower compared with that of the control group, whereas the ultimate load of the HLS group was not significantly changed could be an evidence of the existence of different mechanisms.

The effect of capsaicin on sensory neurons varies with age, strain, and species. Ding et al [21] used a single dosage of 150 mg/kg to treat rats and achieved a 16.9% decrease in BV/TV in the proximal trabecular bone. Offley et al [20] used a dosage of 125 mg/kg to treat rats once every 2 weeks for 4 weeks, and the BV/TV was reduced by 28%. In addition, the present study used the same dosage as that used by Offley et al [20], but the animals were treated four times; this resulted in a 40% reduction in BV/TV. These findings imply that the effect of capsaicin on bone might be dose- and duration-dependent. The dosage and duration should also be taken into consideration while evaluating the effect of capsaicin treatment.

In conclusion, capsaicin-sensitive sensory neurons play an essential role in bone remodelling. While the reduction of bone density is similar between capsaicin treatment and HLS groups, the different bone microarchitecture and biomechanical properties results in capsaicin and disuse groups imply that capsaicin-sensitive sensory neurons are not the sole mechanism of induced bone loss.

Conflicts of interest

The authors declare no conflicts of interest.

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