2	The Influence of High-Heeled Shoes on Strain and Tension
3	Force of the Anterior Talofibular Ligament and Plantar Fascia

- 4 during Balanced Standing and Walking
- 5

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30 Abstract

High-heeled shoes have the capability to alter the strain and tension of ligamentous structure between the foot and ankle, which may result in ankle instability. Contrarily, high-heeled shoes can also reduce the strain on plantar fascia, which may be beneficial to the treatment of plantar fasciitis. In this study, the influence of heel h eight on the strain and tension force of the anterior talofibular ligament (ATL) and plantar fascia were investigated.

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A three-dimensional finite element model of coupled foot-ankle-shoe complex was constructed. Four heel heights were studied in balanced standing: (0-inch, 1-inch, 2-inch, and 3-inch). A 2 inch high-heeled shoe was used for the study during walking stance.

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During balanced standing, the tension force on the ATL increased from 14.8N to 43 44 97.0N, with a six-fold increase of strain from 0 inches to 3 inches. Conversely, at 3 45 inches, the tension force and average strain on the fascia reduced from 151.0N (strain: 0.74%) to 59.6N (strain: 0.28%), and increased sharply to 278.3N (strain: 1.33%) 46 47 despite it being less relative to standing. The walking simulation showed that the fascia tensed while the loading of ATL decreased during push off. The simulation 48 outcome demonstrated the influence of heel height on the alteration of the ATL and 49 50 plantar fascia strain, which has risk implications for ankle injury and also guidance for 51 the treatment for plantar fasciitis.

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### 53 Keywords:

54 Finite element analysis; High-heeled shoe; Foot and Ankle; Sprain ankle; plantar 55 fasciitis

56 Introduction

Presently, high-heeled shoes (HHS) are more than just sensuous fashion; they can be seen as indispensable articles in the lives of many. The majority of females wear HHS, of which, nearly half of them wear HHS daily[1]. However, HHS are considered to be the major cause of foot pain and source of pathologies in women[2]. The increase in heel height attenuates normal gait and posture, resulting in pain, discomfort and impaired foot functions[3]. HHS are also viewed as the major culprits for hallux valgus and calluses[3].

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Ankle injuries, such as ankle sprains, are associated with an increased heel height, which predisposes the risk of inversion injury through excessive ankle plantarflexion and inversion[4, 5]. The altered ankle kinematics causes compensation at the knee joint, including significant increase in knee joint angle and abduction moment[6]. The overall change in gait kinematics produce muscle fatigue and imbalance in the gastrocnemius muscles, which eventually bring about ankle and walking instability[7, 8].

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73 On the contrary, appropriate heel height is beneficial in the treatment of plantar fasciitis[9]. Decreased plantar fascia strain was demonstrated in cadaveric study[10] 74 75 and finite element (FE) simulation[11]. The reduced contact area between the heel and forefoot, together with the raised heel height, was believed to contribute to reduced 76 fascia strain[10]. Besides, HHS significantly increases ankle plantarflexion angle, 77 78 reduces postural stability, increases lower limb muscle forces and shifts plantar pressure anteriorly[3, 4]. In fact, the intrinsic influence of heel height on the 79 ligamentous structure could provide insight to the mechanism of injury and treatment. 80 81 While biomechanical information of the foot and ankle is difficult to obtain from 3 / 17

experiments alone, researchers have identified that a validated computational model
based on FE methods can yield realistic simulations of foot structures, thus providing
pertinent biomechanical information of the foot and ankle [12].

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This study will extend our previous work on the biomechanics of HHS during standing position [11, 13]. The objective of this study is to investigate the effect of heel height on the ligamentous structure, particularly the lateral ankle ligament and plantar fascia during balanced standing and walking stance via FE analysis. Based on the effects of HHS on ankle injury and treatment of plantar fasciitis, it was hypothesized that the strain and tension of the anterior lateral ankle ligament would increase while the strain and tension of the plantar fascia would decrease with the elevation of heel height.

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#### 94 Methods

#### 95 Model Construction

96 The model construction in this study was reported in our previous work[11, 13]. The 97 model was reconstructed from coronal MR images of the right foot in a neutral, non-weight-bearing condition fixed by an ankle-foot orthosis. The images were 98 99 obtained at 1-mm interval using a 3.0-T MR scanner (Siemens, Erlangen, Germany). The subject was a healthy 28 year old female, who is 165 cm tall and has a mass of 100 101 54 kg. The geometry of 28 bony segments and encapsulated soft tissue were segmented by Mimics v14 (Materialise, Leuven, Belgium) and processed by 102 Rapidform XOR2 (3D Systems Korea Inc., Seoul, Korea), as shown in Figure 1. 78 103 ligaments, 9 extrinsic muscles and the plantar fascia were included and modeled by 104 connecting the corresponding attachment points on the bones. The insertion sites of 105 ligaments and muscular structures were referenced to 3D anatomy atlas software: 106 107 Interactive Foot and Ankle (Primal Picture Ltd., London, UK, 2001).

FE package, ABAQUS v6.11 (Dssault Systèmes, RI, USA) was used for mesh creation and subsequent analysis. The bony structures and encapsulated soft tissue were meshed into 4-noded tetrahedral elements (C3D4). Plantar fascia and ligaments were modeled as tension-only truss elements. The articular cartilage was modeled by assigning non-linear contact stiffness between joints[14], which was adopted from a cadaveric study[15]. The articular joints were assumed frictionless, while the coefficient of friction between the ground and encapsulated soft tissue was 0.6[16].

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#### 117 Load and Boundary Conditions

The superior surfaces of the encapsulated soft tissue, distal tibia and distal fibula were fixed. Ground reaction force (GRF) and inclination angle were assigned under the ground plate (Figure 2a). During balanced standing, a vertical GRF of half body weight (270 N) was applied at the inferior surface of foot supports.

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123 The boundary and loading conditions of walking stance were determined from gait analysis of the same subject. Extrinsic muscles were assigned with different 124 magnitudes of muscle forces detailed in our previous work[13]. With the assumption 125 that the soleus and gastrocnemius predominate the propulsion torque during 126 high-heeled gait[17, 18], the muscle force profile of barefoot walking was adopted in 127 128 all heel height conditions except the Achilles tendon load[11]. The Achilles tendon forces were estimated based on a sensitivity analysis[11] on the center of pressure 129 and previous EMG study [19]. The muscle force profiles for all conditions are 130 presented in Table 1. The simulations were repeated in four height values: 0 inches, 1 131 inch, 2 inches and 3 inches in the standing condition. Walking stance was simulated 132 133 only on the 2-inch HHS. The HHS consisted of a sole, heel, shankpiece and upper 5 / 17

134 component[20].

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#### 136 Experimental Validation

The validation was conducted by comparing the plantar pressure distribution and arch 137 138 deformation between experiments and simulations in standing position (Figure. 2b). 139 From the FE analysis, the contact pressure between the plantar foot surface and the 140 ground was extracted to calculate the center of pressure, and compared to the F-scan measurement. The validation process and findings were described in our previous 141 work and acceptable agreement was demonstrated[11, 13]. To summarize, the 142 maximum deviation of the center of pressure in all heel heights between FE 143 144 predictions and measurements were less than 3 mm in the anterior-posterior direction and 2 mm in the medial-lateral direction. 145

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### 147 **Results**

#### 148 High-heeled Shoe Balanced Standing

149 Figure 3a displays the relationship between heel height and tension force in the ATL and total plantar fascia. In the ATL, the tension force increased from 14.8N to 97.0N 150 151 with elevation in heel height from 0 inches to 3 inches. For plantar fascia, the tension force decreased to 59.6N for the 2-inch heel height and increased sharply to 278.3N 152 with 3-inch heel height. The average strain of the plantar fascia reduced from 0.74% 153 to 0.28%, and sharply increased to 1.33% at 3 inches. In the 2-inch condition, the 154 155 strain and total tension force of plantar fascia was minimal in all simulated cases. In 156 particular, the contribution of different plantar fascia rays for tension loading were different. Figure 3b shows the strain of each plantar fascia ray under different heel 157 height conditions. The first and second ray sustained a larger portion of tension. The 158

first ray sustained 36.2% of load for all five rays in the 0-inch heel height situation. On
the contrary, the fifth ray sustained 8.1% in the 0-inch heel height situation.

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#### 162 High-heeled Shoe Walking

For 2-inch high-heeled walking, there was an apparent increase in the tensile strain and tension force of the plantar fascia from 42.7N to 258.4N. Conversely, the change of tension force of the ATL was small from heelstrike to midstance as it decreased at push off (Figure 4). The FE simulation also showed that the tension force of the calcaneofibular ligament (CFL) was negligible during high-heeled walking.

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#### 169 **Discussion**

Biomechanical knowledge of the foot and ankle is important for addressing foot biomechanics and the mechanism for foot and ankle injuries [12, 21]. To overcome the limitations of in vivo experiments, comprehensive computational foot and shoe models can be used to estimate the internal stress and strain of the foot, providing further understanding on foot problems and evaluation on interventions[22].

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176 Footwear can reshape the biomechanics of the foot. Both positive and negative influence of extraordinary footwear was documented in literatures [23-25]. HHS could 177 be considered one of the abnormal designs that are commonly worn but believed to 178 be deleterious. It was proposed that foot pathologies are related to intrinsic factors 179 180 [26-28], while a quantitative evaluation of the extrinsic factors (HHS) is also required 181 to facilitate better footwear design. In this study, the influence of high heels on the 182 ligamentous structure and ankle instability was investigated. Our previous simulations overcame the challenges in the large deformation induced by HHS[11, 20]. Meanwhile, 183

184 further interpretations and simulation on stance were carried out.

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#### ATL strain and tension force 186

The ATL is the most important stabilizer of the talocrural joint. However, it is the 187 188 ligament that undergoes the most damage in a lateral ankle sprain injury. The ATL 189 prevents anterior displacement, as well as any excessive inversion and internal 190 rotation of the talus relative to the tibia. Injuries occurs when the load exceeds the inversion restraint of ATL, especially under compressive loading[29]. Prolonged 191 plantarflexion of the ankle causes tension in the ATL [30], predominantly from neutral 192 position to 20° plantarflexion[31]. Our prediction showed that 3-inch heel height would 193 194 facilitate 25.7° of ankle plantarflexion, in addition to the six-fold increase of predicted strain from 0- to 3-inch heel heights. 195

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#### Plantar fascia strain and tension force 197

198 In this study, the predicted peak strain of plantar fascia reduced when the heel was 199 elevated, but increased sharply from 2-inch to 3-inch heel heights during balanced standing. With respect to high-heeled walking, there was a gradual increase of fascia 200 201 strain from heel strike to push off. Nevertheless the strain was relatively less compared to standing. The findings were in alignment with previous studies [9, 32]. 202 The prediction of load sustained by fascia was 49.2% (applied load), which was 203 204 comparable to 45% reported by Cheung et al.[32] during balanced standing on a flat support. The relationship between fascia strain and heel height was also shown in a 205 206 cadaveric experiment [10].

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A common strategy to treat plantar fasciitis is to reduce the strain in the plantar fascia 208 209 by elevating the heel with shoe modifications or inserting arch insoles [9, 33, 34]. The trend in fascia strain demonstrated in this study showed that an appropriate heel height would be necessary to reduce fascia strain. While in standing position, the predicted total plantar fascia tension force decreased by 77.3%, from 132.8N to 30.1N from 0-inch to 2-inch heel height during balanced standing, respectively. Reduced tensile strain in the plantar fascia may contribute to pain alleviation and reduced inflammation from plantar fasciitis, which is consistent with the treatment outcome of plantar fasciitis[9].

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## 218 Limitations and Suggestions

The external validity of this study was limited due to the single-subject design. Also, there could be possible interactions between the foot anthropometry (such as foot length) and heel heights. Furthermore, the shank profile designs of the high-heeled shoes could produce different supporting forces to the plantar fascia and should be investigated in future studies.

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#### 225 Conclusion

Elevated heel height could significantly change foot biomechanics, especially the strain of the ATL and plantar fascia during balanced standing or walking. In this study, the strain and tension force of the ATL increased with the increase of heel height, while the strain and of plantar fascia decreased at moderate heel height.

230

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# 323 Tables

Table 1 Boundary, loading conditions and muscle load profiles of the subject weighing

325 54kg during balanced standing and stance in different heel heights.

	Balanced Standing				Heelstrike	Midstance	Push-off
Heel Height	0-inch	1-inch	2-inch	3-inch	2-inch	2-inch	2-inch
Tibial inclination	0°				-4°	0°	19°
Vertical GRF	270N			615 N	513N	648N	
Achilles tendon	202.5N	175.5N	216N	432N	405N	594N	756N
force							
Other extrinsic	EHL (10N)				TA (80N)	TA (80N)	FHL (100N)
muscles	EDL (5N)				TP (30N)	PB (50N)	FDL (25N)
PB (20N)				PL (70N)	TP (80N)		
PL (25N)					PB (80N)		
							PL (100N)

326 GRF: Ground Reaction Force; EHL: Extensor Hallux Longus; EDL: Extensor Digitorum Longus; PB:

327 Peroneus Brevis; PL: Peroneus Longus; TA: Tibialis Anterior; TP: Tibialis Posterior; FHL: Flexor Hallux

328 Longus; FDL: Flexor Digitorum Longus

## **Figure Legends**

**Fig. 1** Finite element model of female foot and high-heeled shoe: a) Demonstration of the ATL and plantar fascia in the foot model; b) Demonstration of the foot model embedded in the encapsulated soft tissue aligned with the 2-inch high-heeled shoe during midstance; c) Display of the whole high-heeled shoe model, including the heel, support and upper, with the bony and ligamentous structure of the foot.

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**Fig. 2**(a) boundary and loading condition during stance; (b) Demonstration of validation experiment of the same volunteer on a 2-inch heel support.

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**Fig. 3** Tension force and strain of ATL and plantar fascia (PL) during balanced standing on 0 to 3 inch heel height supports: a) tension force; b) strain.

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Fig. 4 Tension force and strain of ATL and plantar fascia (PL) during 2-inch high-heeled walking: a) tension force; b) strain.



b)



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