
**Title: Biomechanical Comparison of Modified Calcanail System with Plating Fixation
in Intra-articular Calcaneal Fracture: A Finite Element Analysis**

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Abstract

Calcanail system is a novel intramedullary approach for calcaneal fractures but is believed to be insufficient to treat complex fractures. We propose a modified Calcanail technique by adding a transfixation screw to improve stability. The aim of this study was to evaluate the biomechanical stability of the modified Calcanail system and compare it with the traditional Calcanail system and plate fixation. A Sanders type-IIIAB calcaneal fracture model was built and simulated fixation with the three implants. A vertical loading of 700 N was applied to the subtalar joint surfaces, and the posteroinferior calcaneal tuberosity was fixed. Construct stiffness, fracture migration, and von Mises stress were assessed. The results showed the modified Calcanail system demonstrated the highest construct stiffness, smallest migration, and lowest von Mises stress among three fixations. The study suggested that the modified Calcanail system can provide comparatively sufficient stability, that makes it preferable to treat complex calcaneal fractures.

Keywords: Calcaneal fracture; Fracture fixation; Intramedullary nail; Locking plate; Biomechanics; Finite element analysis

1. Introduction

Calcaneal fractures are the most common tarsal bone fractures, and more than two-thirds of them are displaced intra-articular calcaneal fractures (DIACFs) [1]. The DIACF is characterized by the sagittal and coronal fracture lines that divide the calcaneus into anterolateral and superolateral fragments. Patients with DIACFs often have a poor functional outcome, particularly after improper treatments. In extreme case, some of them were handicapped for three years and partially disabled for five years [2]. In fact, the management of a calcaneal fracture is highly complex, and there were debates on the ideal surgical methods [3, 4].

Open reduction and plate fixation could result in a complication rate over 30% [5]. The complications were mostly attributed to the large lateral incision. Surgeons thus switched to minimally invasive techniques in treating DIACFs. Both Kirschner pins and cannulated screws have been clinically used to fix DIACFs [6]. Good clinical results were shown for certain types of fractures, particularly when the reduction was monitored arthroscopically [7]. However, a large number of inadequate reductions and redisplacements occurred when this technique was applied to more comminuted DIACFs [2, 8]. Some cadaveric studies also criticized the biomechanical stability and reduction accuracy of minimally invasive techniques [9, 10].

Recently, a new implant, the Calcanail® system, which uses a novel intramedullary nail, was introduced to treat DIACFs using an intrafocal reduction approach [11]. This implant is composed of a hollow nail and two locking screws, as shown in **Figure 1**. The geometry of the implant was claimed to enhance angular stability, reduction precision, and fixation

strength. The working channel of the implant can accommodate bone grafts and facilitate bone union. The preliminary clinical results of the Calcanail system were positive [12-14]. Biomechanical tests were also conducted to compare its primary stability with other techniques [15, 16].

While the design of the Calcanail system was appreciated, some physicians concerned about its indications and stability to accommodate complex fractures [17]. In this study, we proposed a modified Calcanail technique by combining Calcanial with lag screw fixation. Placing a transfixation screw into the Calcanail channel to hold the anterior process to the main part of calcaneus will help to improve its stability for complex fractures. The plan was inspired by an adjuvant fixation to treat calcaneal fractures using a longitudinal screw [18].

The objective of this study is to determine the biomechanical stability of the Calcanail system and the modified Calcanail system using a transfixation screw in treating complex calcaneal fractures, and to compare them with the traditional plating fixation using finite element analysis (FEA). FEA can provide a versatile platform to evaluate surgical interventions in a controlled environment and to simulate different adverse conditions [19]. It has been commonly used to evaluate the biomechanics of the foot and ankle clinically, such as understanding the mechanism of pathologies and trauma [20], evaluation of foot support [21], implant and fixators [22-23].

2. Materials and methods

2.1 Geometry Reconstruction

The right foot of a male cadaver was scanned by computed tomography (Brilliance 64, Philips Electronics, Netherlands) for the reconstruction of calcaneus geometry. The subject was 62 years old, 170 cm tall, and weighed 70 kg. Ethical approval was granted by the Ethnic Committee of Shanghai Pudong New Area Peoples' Hospital (No. 2017-21). The scan was taken in the transverse direction at 0.75 mm intervals and at 0.54-mm/pixel resolution. The calcaneus bone geometry was reconstructed based on the segmentation of the clinical images using Mimics 15.0 (Materialise, Leuven, Belgium) and a 2.68-mm thick cortical layer was segmented from the trabecular core [24].

The geometry of three implants (Calcanail system, modified Calcanail with transfixation screw, and plate fixation) were reconstructed according to manufacturers' specifications [13] using computer-aided design software Solidworks (Dassault Systèmes Solidworks Corp., MA, USA). The Calcanail implant (FH Orthopedics, Heimsbrunn, France) has a 10-mm diameter and 50-mm-long hollow nail, with slot on both sides and locking screws on both ends (**Figure 1**). The modified Calcanail system was realized by inserting a 3.5-mm diameter transfixation screw through the slot of the Calcanail implant. Plate fixation was carried out with a calcaneal locking plate (Synthes, Solothurn, Switzerland) and screws with simplified cylinders of 3.5-mm diameter.

A Sanders type-IIIAB calcaneal fracture was mimicked according to the model described by Smerek et al [11], with a V-shaped fracture line near the angle of Gissane and two 0.1-mm gaps on the posterior facet fragment. The implants were positioned and aligned

according to the product guidelines [14] and clinical experience (**Figure 2**), which was conducted by an orthopedic surgeon. The bone region which overlapped with the implant was removed using the Boolean operation with the implant.

2.2 Material Properties and Mesh Creation

The material properties were assigned according to previous reports [25-27] and are listed in **Table 1**. Linear tetrahedral elements (C3D4) were created by Abaqus 6.14 (Dassault Systèmes, Paris, France) on the calcaneus bone and implants. The intact calcaneus bone was meshed with 135489 elements. There were 17945, 1170 and 46775 elements in the Calcanail implant, transfixation screw and the plate respectively.

2.3 Boundary and Loading Conditions

The coefficient of friction of the bone-implant interface was assigned 0.3 [26], except for the bone-screw interaction that was fully bonded. A vertical loading of 700N force was applied to the surface of the posterior subtalar joint to simulate single stance standing. The posteroinferior portion of the calcaneal tuberosity was bonded to a polymethylmethacrylate (PMMA) holder to maintain the bone in position [23].

2.4 Data Analysis

The FE analysis was conducted using Abaqus 16.4 (Dassault Systèmes, Waltham, USA). The biomechanical stability was represented the construct stiffness and fracture gap enlargement (migration). The construct stiffness was defined by the ratio of the maximum vertical displacement of the calcaneus to the applied load. The fracture migration was calculated by measuring the distances of 16 pairs of points, which located at the midpoints

and junctions along the fracture line. The average distance change of 16 pairs of points before and after loading was regarded as the fracture migration [28]. In addition, the von Mises stress distribution of the implant would be examined to speculate sites of stress concentration.

2.5 Model Validation

To validate the model, a cadaveric experiment was conducted using the same specimen of the FEA and the vertical stiffness of the experiment was compared with that of the FE prediction. The cadaveric experiment followed the same configurations as that of the simulation, including the creation of the fracture and fixation. The calcaneal posteroinferior tuberosity was bonded to a PMMA holder and 700N vertical loading was applied to the surface of the posterior subtalar joint, which were as same as the simulation.

3. Results

3.1 Construct Stiffness and Validation

Table 2 shows the construct stiffness predicted from the simulations of the three implants. The modified Calcanail system fixation provided the highest stiffness (552 N/mm), followed by the Calcanail system (522 N/mm), and that of the plate fixation was the weakest (454 N/mm). The modified system was 5% and 18% better than the Calcanail system and traditional plate fixation respectively.

With respect to the validation, computer simulations in this study showed good agreement with the cadaveric study. The construct stiffness of the cadaveric model was 450 N/mm, which was comparable to the FE model (454 N/mm). The small differences may be due to the simplification of locking screws in FE analysis.

3.2 Fracture Migration

The migration distances of the three models are also shown in **Table 2**. The inclusion of the lag screw in the modified Calcanail system can provide a higher fracture-stabilizing ability compared with the Calcanail implant alone.

Based on observation, both the Calcanail fixation and its modified technique had a larger mediolateral gap enlargement at the subtalar posterior facet (**Figure 3 (a)**). Conversely, the plate fixation had a larger anteroposterior gap enlargement between the fragments (**Figure 3(b)**). The results demonstrated that the Calcanail system had better stability in the sagittal plane, whereas the plate fixation was more stable in the coronary plane.

3.3 von Mises Stress

The stress distributions of the three implant conditions are illustrated in **Figure 4**. In both the Calcanail and modified Calcanail fixations, the peak stresses were concentrated at the slot of the implant, which was adjacent to the primary fracture line of the calcaneus. On the other hand, stress concentrations for the plate fixation were found at the posterosuperior and anterior parts of the implant, particularly at the plate-screw junction. The stress distribution on calcaneus was similar under three fixations. The stress was concentrated at the medial side, especially in the posterior fracture line of V-shaped angle, as shown in **Figure 5**.

The peak von Mises stresses of the implant and calcaneus cortical/trabecular are plotted in **Figure 6**. The maximum stresses of the Calcanail, modified Calcanail and plate construct were 98.12 MPa, 84.78 MPa, and 102.68 MPa, respectively. Generally, the modified Calcanail system had the lowest peak stress on the implant among the three implant conditions. The peak stress was approximately 17.4% less than that of the plate. Conversely, the plate fixation increased the cortical stress drastically and reduced the trabecular stress slightly. The stress of the cortical bone with the plate fixation was approximately 45% higher than that of the Calcanail system and the modified Calcanail system.

4. Discussion

The use of the Calcanail fixation for calcaneal fractures is a novel surgical option. This approach can maintain the calcaneal height and width to facilitate early rehabilitation and reduce the risk of complications induced by the large incision. Clinical studies revealed favorable outcomes using the Calcanail system [12-14]. However, its capability to accommodate complex fractures, especially those involved anterior process and calcaneocuboid joint fragment was still been challenged. C-Nail was another intramedullary nail system, but up to nine screws would increase the operative complexity [16]. Transfixation screw fixation was a simple and effective tool to improve the fixation stability. For this reason, a modified technique using a lag screw with the Calcanail system was proposed, and its biomechanical performances were assessed and compared with the locking plate and the Calcanail system alone. The results of this study showed that the modified Calcanail system greatly improved the calcaneal fracture fixation stability, and potentially promote fracture union.

From the biomechanical point of view, the structural design of the Calcanail system contributes to better axial stability, whereas that of the calcaneal plate provides better lateral support. This perspective was supported by our findings regarding the fracture migration. In this study, the modified Calcanail technique demonstrated the smallest migration, representing better construct stability. This result was advocated by Wang's studies [18], where adding a transfixing screw can significantly enhance the fixation strength for calcaneal fractures. For the Calcanail system alone, the nail was designed to provide the fixation in one plane and maybe insufficient for comminuted fractures. This would limit the application of the Calcanail system in clinical practice. In this study, the

higher stability and stiffness demonstrated by the modified technique can supplement the insufficiency of the Calcanail alone, and would allow a wider usage including displaced and depressed calcaneal fractures or patients with severe osteoporosis. The modified Calcanail fixation also allows earlier rehabilitation of injured foot, with a lower risk of secondary loss of reduction under partial weight-bearing. In addition, rapid and better fracture union is anticipated with more stable fixation techniques [18].

Construct stiffness is a major determinant to fracture site motion that affects the progression of fracture healing [29]. It was used in cadaveric studies to evaluate the fixation methods for calcaneal fractures [30]. Despite, the reported stiffness values could vary depending on the experimental configurations [29], and thus the interpretation of construct stiffness remains challenging and inconclusive. Smerek et al commented that plate and percutaneous fixation had comparable construct stiffness though there were significant difference with a deviation of 45 N/mm [9]. On the other hand, Rausch et al. found that the augmented screw osteosynthesis was superior to that of the fixed angle locking plate osteosynthesis with about 83 N/mm increase in construct stiffness [31].

Stress distribution is an important indicator representing risk of implant failure. The modified Calcanail fixation experienced the lowest stress compared with the other models. Some stresses may be shared by the transfixation screw, and thus less stress was born by the Calcanail. The plate fixation condition demonstrated the highest stress and was concentrated at the posterosuperior part of the plate and the plate-screw junction. The stress concentration at the plate-screw junction represented a potential risk for hardware failure. Customized stiffness in different portions of the implant could be an alternative to alleviate stress concentration and prevent implant fatigue. Nevertheless, it is worth noting that the

magnitude of the stresses did not exceed the ultimate strength of the implant material, titanium (750–900 MPa), thus suggesting that the construct for all fixations could be primarily safe [32].

Adequate fracture migration at the fracture site could assist in the bone-healing process. Claes et al [33] demonstrated that fracture migration between 0.15 mm and 0.40 mm can assist in the healing of a fracture gap less than 3 mm. In this study, we simulated a joint depressed calcaneal fracture with three fragments and two gaps of 0.1 mm in the posterior subtalar fragment. The relative micro-movement under the normal standing of these bone fragments was less than 0.1 mm (Calcanail and modified Calcanail) and 0.1 mm (plate). Our predicted migration distance was within a range in which in vivo bone regeneration can be expected.

There are some limitations in this study. First, only axial loads were applied to the calcaneus for finite element analysis. The calcaneus, in reality, is exposed to complex forces and moments during walking [34, 35]. Second, soft tissues and other adjacent structures were not included in the models. Finally, the material properties of the calcaneal bone were assumed to be isotropic and linearly elastic. Despite this, the computational model in this study was comparable to those in previous in vitro studies. We believed that the finite element model should be adequately reliable to evaluate the effects of the three fixations. We recommend further biomechanical and clinical studies to validate the findings and explore novel protocols.

5. Conclusions

242 The present study demonstrated that the Calcanail system provided better biomechanical
243 stability than the locking plate for a Sanders type-IIIAB calcaneal fracture fixation. Our
244 proposed modification by adding a transfixation screw to the existing Calcanail system can
245 further enhance the fixation strength/stability and decrease stress concentration. The
246 modified Calcanial system should be routinely recommended for calcaneal fractures.

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Conflict of Interests

The authors declare that there are no competing interests

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Ethical approval

This study was granted by the Ethics Committee of Shanghai Pudong New Area Peoples' Hospital (No. 2017-21)

References

- [1] Schepers T, van Lieshout EM, van Ginhoven TM, Heetveld MJ, Patka P. Current concepts in the treatment of intra-articular calcaneal fractures: results of a nationwide survey. *Int Orthop* 2008;32 (5):711-5. DOI 10.1007/s00264-007-0385-y.
- [2] M. Coughlin, C. Saltzman, and R. Anderson, *Mann's Surgery of the Foot and Ankle*, Elsevier, Amsterdam, Netherlands, 9th Edition, 2014.
- [3] Rammelt S, Zwipp H. Calcaneus fractures: facts, controversies and recent developments. *Injury* 2004;35(5):443-61. <https://doi.org/10.1016/j.injury.2003.10.006>.
- [4] Agren PH, Wretenberg P, Sayed-Noor AS. Operative versus nonoperative treatment of displaced intra-articular calcaneal fractures. *J Bone Joint Surg Am* 2013;95(15):1351-7. doi: 10.2106/JBJS.L.00764.
- [5] Howard, JL, Buckley R, McCormack R, Pate G, Leighton R, Petrie D, Galpin R. Complications following management of displaced intra-articular calcaneal fractures: a prospective randomized trial comparing open reduction internal fixation with nonoperative management. *J Orthop Trauma* 2003;17(4): 241–9.
- [6] Dorr, MC, Backes M, Luitse JS, de Jong VM, Schepers T. Complications of Kirschner Wire Use in Open Reduction and Internal Fixation of Calcaneal Fractures. *J Foot Ankle Surg*, 2016;55(15): 915–7. <https://doi.org/10.1053/j.jfas.2016.04.003>
- [7] Rammelt S, Amlang M, Barthel S, Gavlic JM, Zwipp H. Percutaneous treatment of less severe intraarticular calcaneal fractures. *Clin Orthop Relat Res* 2010;468(4): 983-10. doi: 10.1007/s11999-009-0964-x.

-
- 280 [8] Fernandez DL, Koella C. Combined percutaneous and “minimal” internal fixation for
281 displaced articular fractures of the calcaneus. Clin Orthop Relat Res 1993;290:108-16.
- 282 [9] Smerek JP, Kadakia A, Belkoff SM, Knight TA, Myerson MS, Jeng CL. Percutaneous
283 screw configuration versus perimeter plating of calcaneus fractures: a cadaver study.
284 Foot Ankle Int 2008;29(9):931-5. <https://doi.org/10.3113/FAI.2008.0931>.
- 285 [10] Nelson JD, McIff TE, Moodie PG, Iverson JL, Horton GA. Biomechanical stability
286 of intramedullary technique for fixation of joint depressed calcaneus fracture. Foot
287 Ankle Int 2010;31(3):229-35. <https://doi.org/10.3113/FAI.2010.0229>.
- 288 [11] Goldzak M, Mittlmeier T, Simon P. Locked nailing for the treatment of displaced
289 articular fractures of the calcaneus: description of a new procedure with calcanail. Eur
290 J Orthop Surg Traumatol 2012;22(4): 345–9. DOI 10.1007/s00590-012-0968-1.
- 291 [12] Simon P, Goldzak M, Eschler A, Mittlmeier T. Reduction and internal fixation of
292 displaced intra-articular calcaneal fractures with a locking nail: a prospective study of
293 sixty-nine cases. Int Orthop 2015;39(10):2061-7. DOI 10.1007/s00264-015-2816-5.
- 294 [13] Saß M, Rotter R, Mittlmeier T. Minimally invasive internal fixation of calcaneal
295 fractures or subtalar joint arthrodesis using the Calcanail®. Oper Orthop Traumatol
296 2018: 1-16. <https://doi.org/10.1007/s00064-018-0576-2>.
- 297 [14] Zwipp H, Paša L, Žilka L, Amlang M, Rammelt S, Pompach M. Introduction of a
298 New Locking Nail for Treatment of Intraarticular Calcaneal Fractures. J Orthop
299 Trauma 2016;30(3): 88–92. doi: 10.1097/BOT.0000000000000482.

-
- [15] Goldzak M, Simon P, Mittlmeier T, Chaussemier M, Chiergatti R. Primary stability of an intramedullary calcaneal nail and an angular stable calcaneal plate in a biomechanical testing model of intraarticular calcaneal fracture. *Injury* 2014;45(S1): 49–53. <https://doi.org/10.1016/j.injury.2013.10.031>.
- [16] Reinhardt S, Martin H, Ulmar B, Döbele S, Zwipp H, Rammelt S, Richter M, Pompach M, Mittlmeier T. Interlocking nailing versus interlocking plating in intra-articular calcaneal fractures: a biomechanical study. *Foot Ankle Int* 2016, 37(8): 891-7. <https://doi.org/10.1177/1071100716643586>.
- [17] Wang X, Zhou JQ, Yu GR. Comment on the new calcanail for calcaneus fractures. *Eur J Orthop Surg Traumatol* 2014;22(7):621-2. DOI 10.1007/s00590-012-1021-0.
- [18] Wang CL, Chang GL, Tseng WC, Yu CY, Lin RM. Strength of internal fixation for calcaneal fractures. *Clin Biomech* 1998;13(3):230-3. [https://doi.org/10.1016/S0268-0033\(97\)00042-9](https://doi.org/10.1016/S0268-0033(97)00042-9).
- [19] Wang Y, Wong DW, Zhang M. Computational models of the foot and ankle for pathomechanics and clinical applications: a review. *Ann Biomed Eng* 2016;44(1):213-21. DOI: 10.1007/s10439-015-1359-7.
- [20] Wong DW, Wang Y, Leung AK, Yang M, Zhang M. Finite element simulation on posterior tibial tendinopathy: load transfer alteration and implications to the onset of pes planus. *Clin Biomech* 2018;51:10-6. <https://doi.org/10.1016/j.clinbiomech.2017.11.001>.

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- 320 [21] Yu J, Wong DW, Zhang H, Luo ZP, Zhang M. The influence of high-heeled shoes
321 on strain and tension force of the anterior talofibular ligament and plantar fascia during
322 balanced standing and walking. *Med Eng & Phys* 2016;38(10):1152-6.
323 <https://doi.org/10.1016/j.medengphy.2016.07.009>.
- 324 [22] Wong DW, Wang Y, Chen TL, Leung AK, Zhang M. Biomechanical consequences
325 of subtalar joint arthroereisis in treating posterior tibial tendon dysfunction: a
326 theoretical analysis using finite element analysis. *Comput Methods Biomech Biomed*
327 *Engin* 2017;20(14):1525-32. <https://doi.org/10.1080/10255842.2017.1382484>.
- 328 [23] Ni M, Wong DW, Mei J, Niu W, Zhang M. Biomechanical comparison of locking
329 plate and crossing metallic and absorbable screws fixations for intra-articular calcaneal
330 fractures. *Sci China Life Sci* 2016;59(9):958-64. doi: 10.1007/s11427-016-0010-9.
- 331 [24] Sabry FF, Ebraheim NA, Mehalik JN, Rezcallah AT. Internal architecture of the
332 calcaneus: implications for calcaneus fractures. *Foot Ankle Int* 2000;21(2):114-9.
333 <https://doi.org/10.1177/107110070002100204>.
- 334 [25] Ni M, Weng XH, Mei J, Niu WX. Primary stability of absorbable screw fixation
335 for intra-articular calcaneal fractures: a finite element analysis. *J Med Biol Eng*
336 2015;35(2): 236-41. DOI 10.1007/s40846-015-0019-6.
- 337 [26] Ramlee MH, Kadir MR, Murali MR, Kamarul T. Finite element analysis of three
338 commonly used external fixation devices for treating Type III pilon fractures. *Med Eng*
339 *Phys* 2014;36(10):1322-30. <https://doi.org/10.1016/j.medengphy.2014.05.015>.

-
- 340 [27] Kim SB, Kim YJ, Yoon TL, Park SA, Cho IH, Kim EJ, Kim IA, Shin JW. The
341 characteristics of a hydroxyapatite-chitosan-PMMA bone cement. *Biomaterials*
342 2004;25(26): 5715-23. <https://doi.org/10.1016/j.biomaterials.2004.01.022>.
- 343 [28] Chen SH, Chiang MC, Hung CH, lin SC, Chang HW. Finite element comparison
344 of retrograde intramedullary nailing and locking plate fixation with/without an
345 intramedullary allograft for distal femur fracture following total knee arthroplasty.
346 *Knee* 2014;21(1): 224-31. <https://doi.org/10.1016/j.knee.2013.03.006>.
- 347 [29] Bottlang M, Doornink J, Lujan TJ, Fitzpatrick DC, Marsh JL, Augat P, von
348 Rechenberg B, Lesser M, Madey SM. AAOS Supplement Selected Scientific Exhibits:
349 Effects of Construct Stiffness on Healing of Fractures Stabilized with Locking Plates.
350 *J Bone Joint Surg Am* 2010;92(S2):12-22 doi:10.2106/JBJS.J.00780.
- 351 [30] Dingemans SA, Sintenie FW, de Jong VM, Luitse JS, Schepers T. Fixation
352 methods for calcaneus fractures: a systematic review of biomechanical studies using
353 cadaver specimens. *J Foot Ankle Surg* 2018;57(1):116-22.
354 <https://doi.org/10.1053/j.jfas.2017.05.042>.
- 355 [31] Rausch S, Klos K, Wolf U, Gras M, Simons P, Brodt S, Windolf M, Gueorguiev B.
356 A biomechanical comparison of fixed angle locking compression plate osteosynthesis
357 and cement augmented screw osteosynthesis in the management of intra articular
358 calcaneal fractures. *Int Orthop* 2014;38(8):1705-10. DOI 10.1007/s00264-014-2334-x.
- 359 [32] Sitthiseripratip K, Van Oosterwyck H, Vander Sloten J, Mahaisavariya B, Bohez
360 ELJ, Suwanprateeb J, Van Audekerckeb R, Orisa P. Finite element study of trochanteric

-
- 361 gamma nail for trochanteric fracture. *Med Eng Phys* 2003;25(2): 99–106.
362 [https://doi.org/10.1016/S1350-4533\(02\)00185-6](https://doi.org/10.1016/S1350-4533(02)00185-6).
- 363 [33] Claes LE, Wilke HJ, Augat P, Rübenacker S, Margevicius KJ. Effect of
364 dynamization on gap healing of diaphyseal fractures under external fixation. *Clin*
365 *Biomech* 1995;10(5):227-34. [https://doi.org/10.1016/0268-0033\(95\)99799-8](https://doi.org/10.1016/0268-0033(95)99799-8).
- 366 [34] Racic V, Pavic A, Brownjohn J. Experimental identification and analytical
367 modelling of human walking forces: literature review. *J Sound Vib* 2009;326(1-2):1-
368 49. <https://doi.org/10.1016/j.jsv.2009.04.020>.
- 369 [35] Seipel RC, Pintar FA, Yoganandan N, Boynton MD. Biomechanics of calcaneal
370 fractures: a model for the motor vehicle. *Clin Orthop Relat Res* 2001;388:218-24.